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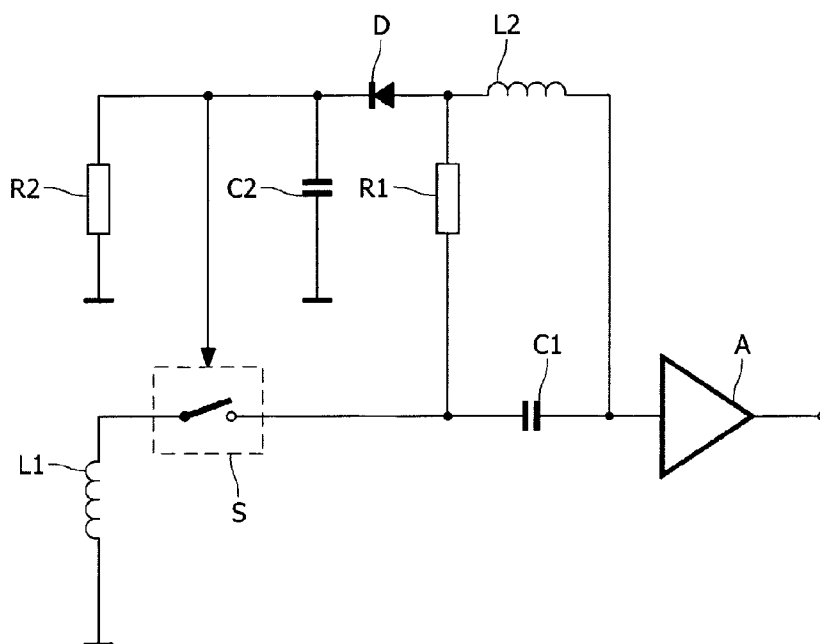
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(54) Title: **CIRCUIT ARRANGEMENT FOR DETUNING A RESONANT CIRCUIT OF AN MR APPARATUS**



(57) Abstract: The invention relates to a circuit arrangement for an MR apparatus, having a resonant circuit, which is formed by an MR receiving coil (L1) and a capacitor (C1), and having an electronic control circuit (S) for switching the resonant circuit between two or more operating modes. The invention proposes that the electronic control circuit (S) be connected with a receiving device (L2) for wireless reception of a high-frequency electromagnetic control signal.

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For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

Circuit arrangement for detuning a resonant circuit of an MR apparatus

The invention relates to a circuit arrangement for an MR apparatus, having a resonant circuit, which is formed by an MR receiving coil and a capacitor, and having an electronic control circuit for switching the resonant circuit between two or more operating modes.

5 The invention also relates to an MR apparatus having a circuit arrangement according to the invention and to an MR method employing such an MR apparatus.

MR apparatuses used primarily for medical imaging purposes are known from
10 the prior art; separate transmitting and receiving coil arrangements are provided in these apparatuses. The purpose of the transmitting coil arrangement here is to generate high-frequency fields in the examination volume of the MR apparatus, which induce nuclear magnetization in the examination volume. The receiving coil arrangements serve to pick up MR signals from the examination volume. The receiving coil arrangements can either be in
15 the form of volume coils, or – for optimization of sensitivity in specific regions of the examination volume – in the form of surface coils, which are placed directly on the body of a patient located in the examination volume of the MR apparatus. Such receiving coils are normally wired up with suitably adapted capacitors, so that each receiving coil has associated with it a resonant circuit of which the resonant frequency is tuned to the proton resonant
20 frequency of the MR apparatus. To induce the nuclear magnetization in the examination volume, high-frequency pulses in the power range of several kilowatts are normally introduced by means of the transmitting coil arrangement. The frequency of the high-frequency pulses is in turn the same as the resonant frequency of the resonant circuits associated with the receiving coils. The high-frequency pulses therefore enter resonantly into
25 the receive-side resonant circuits of the MR apparatus. The result of this is that, on the one hand, the high-frequency energy is undesirably partially absorbed by way of the receiving coil arrangement. On the other hand, the resonant input possibly causes significant heating of or even irreversible damage to the receiving coil arrangement and to the corresponding resonant circuits. When using surface coils, the resonant heating may lead to a risk of injury

for the patient being examined, on whose body the surface coils are placed directly. It is also problematic that the receive-side resonant circuits are customarily connected to sensitive receiver amplifiers, the input stages of which can be damaged by the high-frequency energy introduced in transmit mode. At any rate, the receiver amplifiers are severely overdriven, so that after every excitation by means of a high-frequency pulse the entire receive electronics of the MR apparatus have an undesirably long dead time before the received MR signals can be correctly processed.

In MR apparatuses that have separate transmitting and receiving coil arrangements, it is known specifically to detune the receive-side resonant circuits during transmit mode, so that an input of high-frequency pulses into the receiving coils during transmit mode is prevented. For that purpose, suitable circuit arrangements are provided, by means of which each of the receive-side resonant circuits can be switched back and forth between a resonant operating mode and a non-resonant operating mode. The resonant operating mode is here intended for the receive mode and the non-resonant operating mode is intended for the transmit mode of the MR apparatus.

A circuit arrangement of the kind outlined above is known, for example, from WO 01/74466 A1. The known circuit arrangement serves for switching a resonant circuit having a MR receiving coil in the form of a microcoil between a resonant and a non-resonant operating mode. Here, the entire resonant circuit is mounted at the tip of an intervention instrument. The known circuit arrangement comprises an optoelectronic element, by means of which the resonant circuit is detuned. In the case of the known circuit arrangement, the control signal that causes detuning of the resonant circuit is a light signal, which is fed to the optoelectronic element by way of an optical waveguide.

The drawback of the system known from the prior is primarily the fact that the (optical) control signal has to be fed to the resonant circuit to be switched back and forth between the different operating modes by way of a signal line specifically intended for this. For that purpose, apart from the optical waveguide, yet further optoelectronic components are required, which do not belong to the regular equipment of customary MR apparatuses. As a technically simpler version, it would admittedly be possible for the control signal for switching between the different operating modes to be fed to the resonant circuit in the form of an electrical signal by way of conventional electrical connecting wires. But the problem inherent in this is that suitable electrical connecting wires that connect the reversible resonant circuit of the MR receiving coil to the central control unit of the MR apparatus have to be several meters long. Such long wires in turn act as receiving antennas, which the high-

frequency pulses couple into in transmit mode. Here too, resonant heating phenomena can occur, which represent a corresponding risk of injury for the patient to be examined.

5 Taking this as starting point, it is an object of the invention to provide a circuit arrangement for an MR apparatus for switching a receive-side resonant circuit between different operating modes, wherein the circuit arrangement can be simply and inexpensively realized and can be used without any risk of injury for the patient.

 That object is achieved by the invention by a circuit arrangement as claimed in
10 claim 1, the electronic control circuit being connected with a receiving device for wireless reception of a high-frequency electromagnetic control signal.

 Through the use of a high-frequency electromagnetic control signal, that is, a radio signal, for activating the resonant circuit, any physical connection between the receive-side resonant circuit and the central control unit of the MR apparatus can be omitted. There is
15 no risk of injury for the patient being examined since the high-frequency electromagnetic control signals for switching over the resonant circuit place at least no more stress on him than the high-frequency fields to which he is exposed anyway during the transmit mode of the MR apparatus. The electronic control circuit required to switch over the resonant circuit, together with the associated receiving device for wireless reception of the control signal, can
20 be realized with standard components at low cost. In particular, the expensive optoelectronics that are required in the case of the system known from the above-mentioned printed publication can be omitted.

 An especially practicable version of the circuit arrangement according to the invention is produced as claimed in claim 2 when the receiving device is formed by the MR
25 receiving coil itself, switching over of the resonant circuit being controllable by means of the control circuit in dependence on the amplitude of the high-frequency signal present at the MR receiving coil. By means of the control circuit, the terminal voltage present at the MR receiving coil is detected, and, when a pre-determinable switching threshold is exceeded, the resonant circuit of the MR receiving coil is switched over to the non-resonant operating
30 mode. If in transmit mode of the MR apparatus a high-frequency pulse is input, then this couples first into the MR receiving coil and thus causes the terminal voltage present at the MR receiving coil to exceed the threshold value. After that, switching over into the non-resonant operating mode is effected, so that the resonant circuit and the receiving electronics in connection therewith are protected.

Alternatively, as claimed in claim 3, in the circuit arrangement according to the invention the receiving device can be formed by an additional resonant circuit, which is tuned to a different resonant frequency from the resonant circuit formed by the MR receiving coil and the associated capacitor. To switch the resonant circuit of the MR receiving coil into the non-resonant operating mode, in this version a high-frequency electromagnetic control signal is sent, to be precise, at the resonant frequency of the additional resonant circuit, this frequency differing from the MR resonant frequency. At the same time, the control signal can advantageously have a very low transmitting power, which does not stress the patient in any way. If there are several independent MR receiving coils with associated resonant circuits, these can either each have an additional resonant circuit, which is tuned to a single common frequency of the control signal, so that all receive-side resonant circuits can be switched with a single control signal between the different operating modes. Alternatively, each receive-side resonant circuit can have an additional resonant circuit each having a different resonant frequency, so that by appropriate selection of the frequency of the control signal, individual receive-side resonant circuits can be switched over specifically.

The additional resonant circuit of the last-described version of the circuit arrangement according to the invention can advantageously be connected to a rectifier circuit for generating a low-frequency switch-over signal, as claimed in claim 4. From the high-frequency control signal received by the additional resonant circuit, the rectifier circuit generates the low-frequency switch-over signal that is required within the electronic control circuit of the circuit arrangement according to the invention for switching between the possible operating modes. According to this version, it is advantageous that the energy supply for switching over is applied by the received electromagnetic control signal itself, so that the circuit arrangement according to the invention manages entirely without its own energy supply and without active circuit components.

An advantageous further aspect of the circuit arrangement according to the invention is produced as claimed in claim 5, wherein the control circuit comprises a time-delay circuit that is constructed so that the resonant circuit formed by the MR receiving coil and the associated capacitor, on receipt of the control signal, is switched over into an activated or a deactivated operating mode, and thereafter remains in that operating mode for a time interval of pre-determinable duration. It is thus possible, for example, shortly before the introduction of a high-frequency pulse in transmit mode of the MR apparatus to transmit the control signal in order to switch over the resonant circuit of the MR receiving coil into the non-resonant operating mode. The time-delay circuit ensures that the receive-side resonant

circuit remains in this de-activated operating mode for the duration of the transmit mode of the MR apparatus. Once the transmit mode has ended, the resonant circuit MR receiving coil is automatically switched back into the activated, that is, resonant operating mode.

Alternatively, the circuit arrangement can be constructed so that shortly before the start of the receive mode the resonant circuit is switched by means of the control signal from the non-resonant operating mode intended for the transmit mode into the resonant operating mode, and by virtue of the time-delay circuit remains in this resonant operating mode throughout reception of the MR signals.

In a further possible embodiment of the circuit arrangement according to the invention, as claimed in claim 6 the receiving device is constructed to receive radio signals of a radio control. Commercial radio control components can accordingly be used to realize the invention.

The circuit arrangement according to the invention can be used for an MR apparatus as claimed in claim 7.

In addition, the circuit arrangement according to the invention can be used as claimed in claims 8 and 9 in an MR method to generate an image of an examination object, the image being reconstructed from MR signals that are picked up from the examination volume after input of a high-frequency pulse, and the resonant circuit formed by the MR receiving coil and the associated capacitor being switched by additional generation of a high-frequency electromagnetic control signal between an activated and a de-activated operating mode, such that the resonant circuit is in the de-activated operating mode during input of the high-frequency pulse. Here, as stated above, the control signal may have a different frequency from the high-frequency pulse and in particular the control signal can be generated before or after the high-frequency pulse if the control circuit is equipped with the above-described time-delay circuit.

The method according to the invention can be made available to the user of MR apparatuses as claimed in claim 10 in the form of a corresponding computer program. The computer program can be stored on suitable storage media, for example CD Rom or diskette, or it can be downloaded via the internet onto the computer unit of the MR apparatus.

These and other aspects of the invention are apparent from and will be elucidated with reference to the embodiments described hereinafter.

In the drawings:

Fig. 1 shows the MR apparatus according to the invention;

Fig. 2 shows the circuit arrangement according to the invention.

5 Fig. 1 shows an MR apparatus according to the invention in the form of a block diagram. The apparatus comprises a main field coil 1 for generating a homogeneous, static magnetic field in an examination volume, in which there is a patient 2. The MR apparatus illustrated furthermore comprises gradient coils 3, 4 and 5 for generating magnetic field gradients in different directions in space within the examination volume. By means of a
10 computer unit 6, which is connected via a gradient amplifier 7 to the gradient coils 3, 4 and 5, the variation with time of the magnetic field gradients within the examination volume is controlled. A transmitting coil 8 for generating high-frequency fields in the examination volume also forms part of the MR apparatus. The transmitting coil is in connection by way of a transmitting amplifier 9 with the computer unit 6. An MR receiving coil 10, which is part of
15 a resonant circuit not illustrated in Fig. 1, is used to pick up MR signals from the examination volume. A control circuit, which is symbolized in Fig. 1 by a switch 11, is provided to switch the resonant circuit between two or more operating modes. The switch 11 is activated by a receiving device 12, the receiving device 12 being constructed for wireless reception of a high-frequency electromagnetic control signal. A transmitting unit 13, which in its turn is in
20 connection with the computer unit 6, is used to transmit the control signal. Alternatively, the transmitting coil 8 that is already present can be used for transmitting the control signal. Switching the resonant circuit between the different operating modes is therefore monitored by the computer unit 6. The MR receiving coil is in connection via the switch 11 with a receiving unit 14, which is used to amplify and to demodulate the received MR signals. The
25 MR signals thus processed are transmitted to a reconstruction and visualization unit 15. An image reconstructed from the MR signals can be displayed by means of a monitor 16. The computer unit 6 possesses a program control, by which the above-described MR method can be implemented on the MR apparatus.

 The circuit arrangement illustrated in Fig. 2 comprises a resonant circuit,
30 which is formed by an MR receiving coil L1 and a capacitor C1. An electronic switch S is provided for switching the resonant circuit between two or more operating modes. In a de-activated operating mode, in which according to the invention is it intended to prevent high-frequency radiation from coupling into the resonant circuit, the electronic switch S is open. In this operating mode, above all a sensitive receiver amplifier A is prevented from suffering

damage or at least from being overdriven. In an activated operating mode, the switch S is closed, so that the resonant circuit formed by the MR receiving coil L1 and the associated capacitor C1 is resonant and MR signals can be received. In the case of the circuit arrangement illustrated in Fig. 2, an additional receiving coil L2 is provided as well, and

5 together with the capacitor C1 this forms an additional resonant circuit, which is tuned to a different resonant frequency from the resonant circuit formed by the MR receiving coil L1 and the associated capacitor C1. This additional resonant circuit serves to receive a high-frequency electromagnetic control signal, which has a different frequency from the frequency of the MR signals to be received. The control signal received by means of the additional

10 resonant circuit decays across a resistor R1 and is rectified by means of a diode D. A low-frequency switching signal for switching the change-over switch S is thereby produced. The control circuit furthermore comprises a time-delay circuit, which is formed by a capacitor C2 and a resistor R2. The capacitor C2 is charged by the received control signal. Discharge of the capacitor C2 is effected after termination of the input of the control signal via the resistor

15 R2. The capacitor C2 and the resistor R2 define a time constant, so that, on receipt of the high-frequency control signal, the resonant circuit formed by the MR receiving coil L1 and the associated capacitor C1 is switched by means of the additional resonant circuit firstly into the de-activated operating mode and thereafter remains in that operating mode throughout the time predetermined by the time constant, even when the control signal is no longer present.

20 Alternatively, the circuit arrangement illustrated in Fig. 2 can be constructed so that the change-over switch S is closed by the low-frequency switching signal, so that the resonant circuit for receiving MR signals, formed by the MR receiving coil L1 and the associated capacitor C1, is switched out of the de-activated operating mode into the activated resonant operating mode and then remains in that operating mode throughout the corresponding time

25 interval.

CLAIMS:

1. A circuit arrangement for an MR apparatus, having a resonant circuit which is formed by an MR receiving coil (L1) and a capacitor (C1), and having an electronic control circuit (S) for switching the resonant circuit between two or more operating modes, wherein the electronic control circuit (S) is connected to a receiving device (L2) for wireless reception
5 of a high-frequency electromagnetic control signal.
2. A circuit arrangement as claimed in claim 1, wherein the receiving device is formed by the MR receiving coil itself, and wherein switching over of the resonant circuit is controllable by means of the control circuit in dependence on the amplitude of the high-
10 frequency signal present at the MR receiving coil.
3. A circuit arrangement as claimed in claim 1, wherein the receiving device is formed by an additional resonant circuit which is tuned to a different resonant frequency from the resonant circuit formed by the MR receiving coil and the associated capacitor.
15
4. A circuit arrangement as claimed in claim 3, wherein the additional resonant circuit is connected to a rectifier circuit for generating a low-frequency switching signal.
5. A circuit arrangement as claimed in any one of claims 1 to 4, wherein the
20 control circuit comprises a time-delay circuit that is constructed such that the resonant circuit formed by the MR receiving coil and the associated capacitor, upon receipt of the control signal, is switched over into an activated or de-activated operating mode, and thereafter remains in that operating mode for a time interval of pre-determinable duration.
- 25 6. A circuit arrangement as claimed in claim 1, wherein the receiving device is constructed for receiving radio signals of a radio control.
7. MR apparatus having a main field coil (1) for generating a substantially homogeneous, static magnetic field in an examination volume, a transmitting coil (8) for

generating high-frequency fields in the examination volume, an MR receiving coil (10) for receiving MR apparatus signals from the examination volume, a computer unit (6) for controlling the MR apparatus, and having a circuit arrangement as claimed in any one of claims 1 to 6.

5

8. An MR method for generating an image of an examination object using an MR apparatus as claimed in claim 7, wherein the image is reconstructed from MR signals that are received from the examination volume after input of a high-frequency pulse, and wherein the resonant circuit formed by the MR receiving coil (L1) and the associated capacitor (C1) is
10 switched by additional generation of a high-frequency electromagnetic control signal between an activated and a de-activated operating mode, such that the resonant circuit is in the de-activated operating mode during input of the high-frequency pulse.

9. An MR method as claimed in claim 8, wherein the control signal has a
15 different frequency from the high-frequency pulse and wherein the control signal is generated before or after the high-frequency pulse.

10. Computer program for an MR apparatus as claimed in claim 7, wherein an MR method as claimed in claim 8 or 9 is implemented by the computer program on the computer
20 unit of the MR apparatus.

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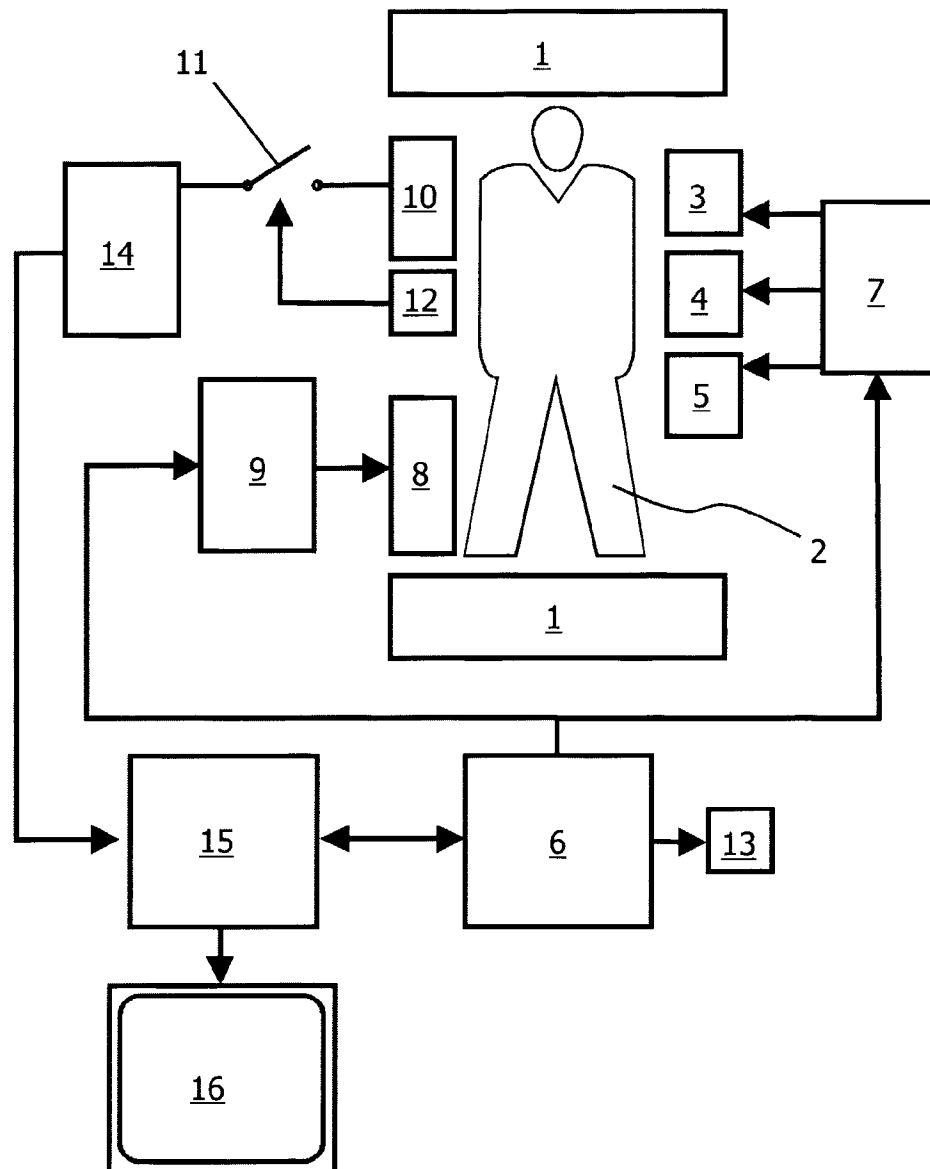


FIG.1

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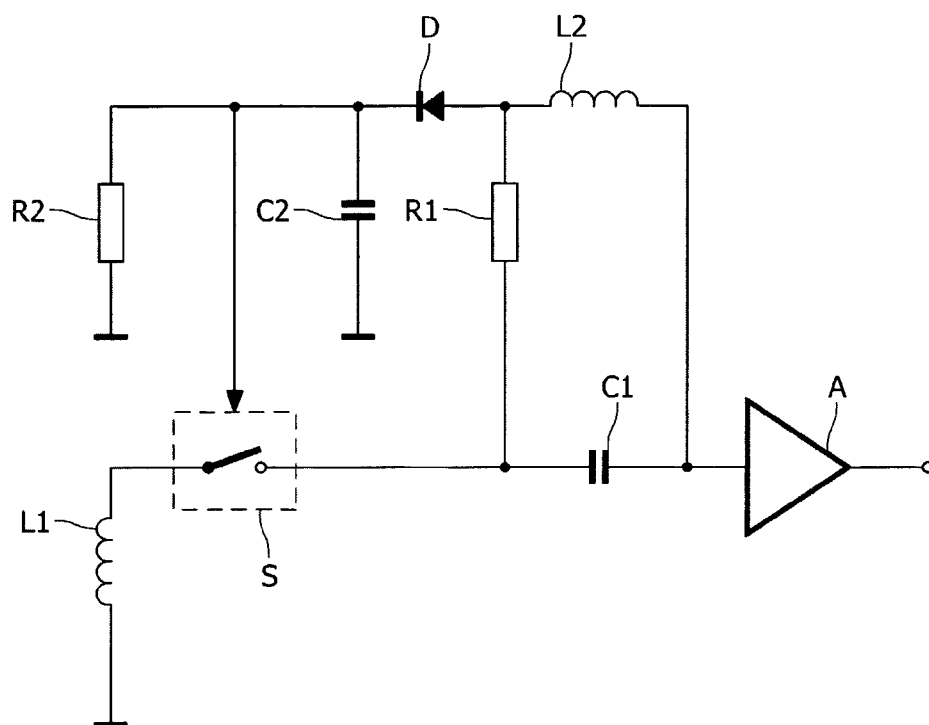


FIG. 2

INTERNATIONAL SEARCH REPORT

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A. CLASSIFICATION OF SUBJECT MATTER

IPC 7 G01R33/36

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 G01R A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, INSPEC, COMPENDEX, MEDLINE, EMBASE, BIOSIS, PAJ, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 6 280 385 B1 (MELZER ANDREAS ET AL) 28 August 2001 (2001-08-28) column 11, line 15 - line 26 column 12, line 42 - line 51; figures 2e-g -----	1,2,5-7, 10
A	WO 01/75466 A (CASE WESTERN RESERVE UNIVERSITY; DUERK, JEFFREY, L; WENDT, MICHAEL; WO) 11 October 2001 (2001-10-11) cited in the application page 11, line 3 - line 25 -----	1-10
A	US 5 162 738 A (SEPPONEN ET AL) 10 November 1992 (1992-11-10) column 3, line 8 - column 4, line 29 -----	1-10



Further documents are listed in the continuation of box C.



Patent family members are listed in annex.

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